

Molecular Imaging: the Latest Generation of Contrast Agents and Tissue Characterization Techniques

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Abstract Molecular Imaging technologies will have a profound impact on both basic research and clinical imaging in the near future. As the field covers many different specialties and scientific disciplines it is not possible to review all in a single article. In the current article we will turn our attention to those modalities that are either currently in use or in development for the medical imaging clinic. *J. Cell. Biochem.* 90: 443–453, 2003. © 2003 Wiley-Liss, Inc.

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The focus of this article will be to review the novel molecular imaging based contrast agents that have the greatest potential for use in clinical medicine in near future. We will discuss how the current modalities that are available for human use namely, computed tomography (CT), magnetic resonance imaging (MRI), ultrasound (US), single photon emission computed tomography (SPECT), or positron emission tomography (PET), and how they can be applied to the imaging of these new contrast agents.

MRI, US, AND CT

To successfully study specific receptor systems it is helpful to understand the cells expressing the receptors and the circumstances leading to changes in expression [Fischman et al., 1989]. Any receptors expressed in sufficient quantity (at least 10–50,000 copies/cell) with sufficiently high affinity for the injected agent ($>10^{-8}$ M) can be detected by external

imaging [Blankenberg et al., 2000; Behr et al., 2001]. In general, radiopharmaceuticals developed for SPECT and PET have (a) high specificity (b) sensitivity requiring, (c) minimal amounts of labeled material ~ 0.1 – 10 nmoles per dose as compared with MRI and US, or iodinated contrast media for CT where concentrations ranging from ~ 10 μ M to ~ 100 μ M are required for imaging. While SPECT and PET offer exceptional sensitivity with respect to the amount of contrast material needed for imaging, they lack the exquisitely high anatomical spatial resolution of US, CT, and MRI. The high sensitivity of SPECT and PET to small amounts of contrast agents and high anatomic resolution with CT and MRI, however, can be combined with the current generation of PET/CT [Ketani and Hartshorne, 2001; Townsend and Beyer, 2002], SPECT/CT [Forster et al., 2003], and soon PET/MRI [Nishioka et al., 2002] clinical scanners in which co-registration of radionuclide and anatomical images (i.e., fusion imaging) is now possible as shown in Figure 1.

A variety of contrast agents have been developed for US, CT, and particularly, MRI. Most MR agents constructed thus far take advantage of either iron particulates or gadolinium (Gd)-compounds to modulate signal at the site or target of interest. Usually multiple atoms of iron or Gd are placed onto targeting molecules of interest either by attachment to polylysine, dextran, dendrimer, or coated liposome to decrease the amount of targeting material required for external imaging [Aime et al., 2002].

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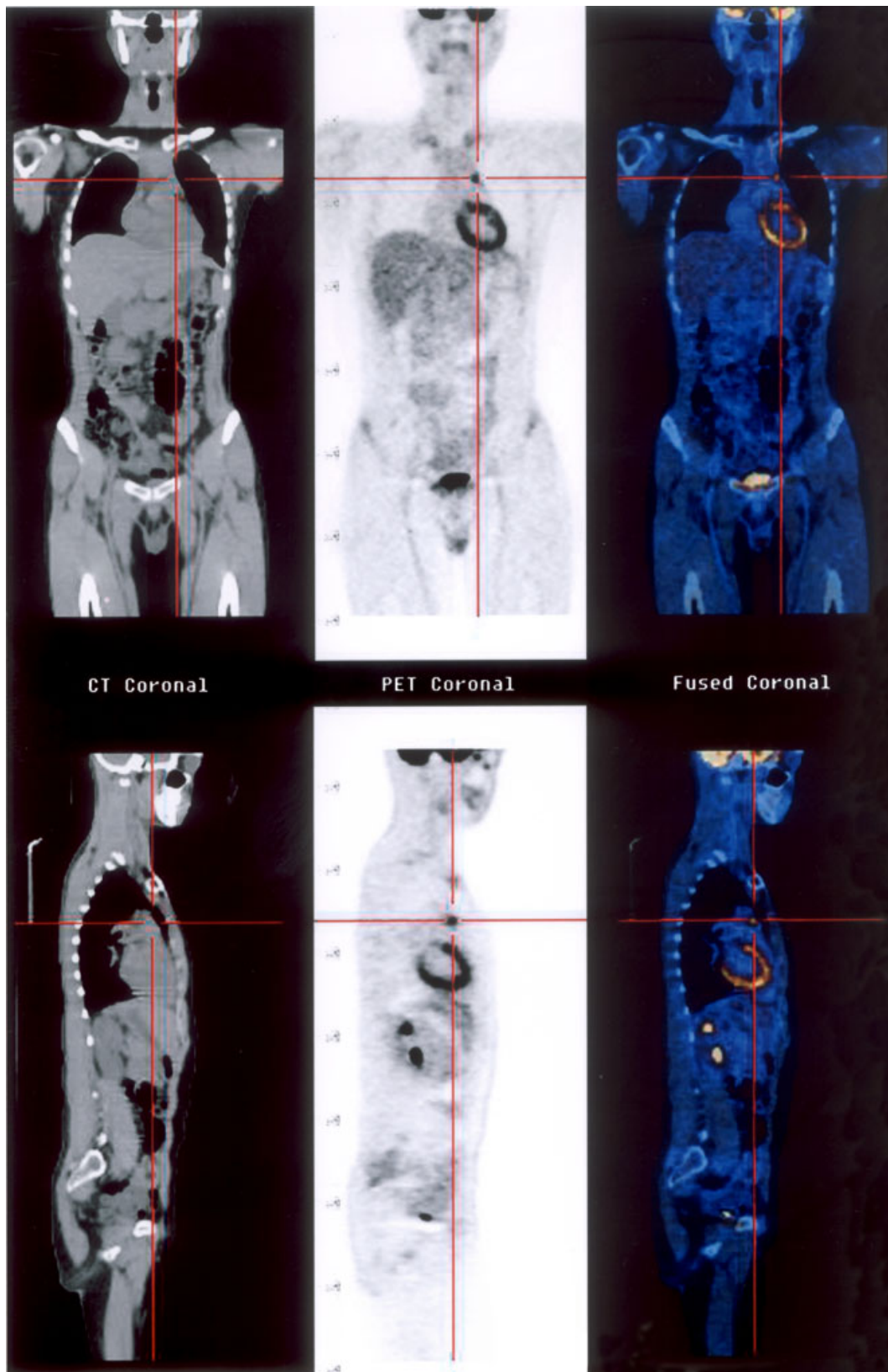


Fig. 1. Positron emission tomography/computed tomography (PET/CT) scanning with ^{18}F -fluoro-deoxyglucose (FDG). Coronal (**above**) and sagittal (**below**) tomographic images of non-enhanced CT, FDG PET, and fusion of CT/PET image data sets are shown in a 50-year-old male with recurrent lung carcinoma involving a <1 cm sized malignant lymph node in the anterior mediastinum marked by cross hairs on all three sets of coronal

and sagittal images. Note the marked focal uptake of FDG within recurrent tumor seen in both the PET and fusion image data sets. Note the non-specific uptake of FDG within the brain heart and kidneys, and to a lesser extent the liver, gut, and blood vessels (i.e., blood pool). [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

Iron nanoparticulates (superparamagnetic iron oxide particles (SPIOs) or ultra-small (USPIOs)) are usually stabilized with aminated-cross linked dextrans for in vivo administration [Kooi et al., 2003; Rydland et al., 2003]. Iron particles act as small permanent magnets that dephase proton spins in the local micro-environment thereby causing a local loss of MR signal in target tissues and cells on T2-weighted MR pulse sequences. At present these iron nanoparticles are used primarily as blood pool or macrophage (liver, spleen, lymph nodes, and bone marrow) imaging agents. Iron particulates, however, can be conjugated to any number of peptides, antibodies, enzymes, or fluorescent probes, and have even been used to track SPIO labeled dendritic cells in vivo [Lewin et al., 2000; Weissleder et al., 2000; Josephson et al., 2002; Lanza et al., 2002]. In near future it should be possible also to image intracellular production of metallomelanin, an iron containing protein whose synthesis is dependent on the expression of tyrosinase, as a part of reporter gene system for MR [Alfke et al., 2003].

Alternatively, Gadopentetate dimeglumine (Gd-DTPA) and other Gd-complexes can also be used to tag molecules of interest for MR imaging. Examples of Gd-based agents include anti- $\alpha_v\beta_3$ -antibody coated Gd-DTPA liposomes for MR imaging of tumor angiogenesis [Sipkins et al., 1998], poly Gd-DTPA or Gadolinium tetra azacyclododecane tetraacetic acid labeled anti-carcino embryonic antigen (CEA)F(ab')(2) fragments that target colorectal carcinoma [Curtet et al., 1998], and Gd-labeled mesoporphyrins for the MR assessment of necrotic non-viable tumor, infarcted myocardium, and soft tissue abscesses [Ju Lee et al., 2002; Lee et al., 2003].

MR contrast agents that generate signal under certain specific physiologic and pathologic conditions are also under development [Aime et al., 2002]. The best characterized of these new micro-environment sensitive MR agents is the Egd-Gd complex [Weinmann et al., 2003]. The Egd-Gd complex is composed of a derivative of Gd-HPDO3A containing a β -galactose moiety that prevents the access of water molecules to the paramagnetic center of the molecule. In the presence of β -galactosidase encoded by the *lacZ* genes, the galactose moiety is removed allowing for the interaction of water molecules with the Gd-core and the enhancement of MR signal on T1-weighted images. Plasmids, constructed to include the gene for

β -galactosidase in addition to those for gene therapy can then be directly imaged in vivo with MR when followed by intravenous injection of Egd-Gd complex. Two other more generalizable enzymatic Gd-based systems have been developed; the first a Gd-DOTA like monomer complex bearing a catechol functionality that in the presence of peroxidase polymerizes into paramagnetic MR detectable oligomeric molecules, and the second, insoluble Gd-DTPA like complexes which when internalized by macrophages are hydrolyzed by intracellular esterases into soluble MR detectable molecules.

The development of novel micro-bubble based contrast agents for US is currently focused on blood pool and macrophage/reticulo-endothelial system (RES) for liver/spleen/lymph node and atherosclerotic plaque imaging [Harvey et al., 2002; Yucel et al., 2002; Hohmann et al., 2003]. Most of these agents are composed of lipid, albumin, or prefluorocarbon shells encapsulating microbubbles $<5 \mu\text{m}$ in diameter permitting easy access to all portions of the microcirculation. Because of their size and physical characteristics these agents are confined to the imaging of the vascular space. There is, however, the potential of directing biotinylated coated microbubbles with a number of avidin labeled molecules including anti-integrin $\alpha_v\beta_3$, anti-P-selectin, and anti-ICAM-1 antibodies [Lanza et al., 1996; Lindner, 2002]. In contrast to MR and US, there has been little progress in beyond the development of lipophilic and nanoparticulate iodinated agents for blood pool, liver, spleen, lymph node, and bone marrow imaging [Choi et al., 1994; Gazelle et al., 1995; Li et al., 1996].

PET AND SPECT RADIONUCLIDE IMAGING

Molecular imaging is the natural outgrowth of the biochemical techniques and radionuclide imaging devices developed over the past several decades for the field of Nuclear Medicine. We in the next section will discuss the most salient of the newer radiopharmaceuticals that are either currently available or in route to the Nuclear Medicine clinic.

Somatostatins

Five different somatostatin receptors (SSTR)-1 through SSTR-5 [Reichlin, 1983] have been described. SSTR-2 appears to be expressed in a majority of human cancers (to varying degrees)

and on activated lymphocytes. SSTR-1, and to a lesser extent SSTR-4, have been reported only in prostate carcinoma, and human normal and hyperplastic endothelium, but not animals where SSTR-2 predominates [Curtis et al., 2000]. Caution therefore, needs to be exercised, as with all translational research, of interspecies differences in receptor type and expression.

Somatostatin itself plays a role in cancer, in particular as a tumor growth inhibitor [Lamberts et al., 1991; Denzler and Reubi, 1999]. The marked SSTR (mostly SSTR-2) density found in breast carcinoma, lymphoma, and neuroendocrine tumors permits clinical SPECT imaging of primary and metastatic tumor with currently available radiolabeled somatostatin analogs namely, ^{111}In -D-Phe-DTPA-octreotide (Octreoscan, Mallinckrodt Medical, St. Louis, MO) [Krenning et al., 1993; Vallabhajosula et al., 1996] and $^{99\text{m}}\text{Tc}$ -depreotide (Neotect, Diatide Inc., Londonderry, NH) [Breeman et al., 2001]. These agents are also now being used for the detection of malignant versus benign lung nodules, as well as pathologic lymphocytic processes such as lymphoma, Graves' ophthalmopathy, granulomatous disease, cardiac allograft rejection, and the formation of unstable (vulnerable) atherosclerotic plaques in which T-lymphocytes accumulate and overexpress the SSTR-2 receptor [Nocaudie et al., 1999; Balon et al., 2001; Cascini et al., 2001; Mari et al., 2001].

The SSTR-2 receptor gene has also been successfully used as a molecular reporter of the incorporation and expression of DNA constructs

in vivo [Zinn et al., 2000]. It is possible that SSTR-2 receptor gene expression (imaged with Octreoscan or Neotect) could also be used as reporter signal in non-viral molecular delivery vehicles recently described by Backer et al. [2002]. This new targeting technology relies on the non-covalent binding of standardized "payload" modules to targeting proteins expressed with a docking tag as shown in Figure 2. The payload modules are constructed by linking drug or DNA carriers to the adapter protein capable of binding to the docking tag. The system described above was originally constructed with fragments of bovine ribonuclease A used as an adapter protein and a docking tag with VEGF₁₂₁ as the internalizable targeting protein, but has been recently humanized for potential clinical use for imaging or drug delivery [unpublished data].

The advantage of this new delivery system is that it avoids the problems of (i) potential inactivation of cell binding domains by conjugation, (ii) inevitable heterogeneity of the final products, (iii) the development of custom conjugation procedures for every targeting protein, and (iv) avoids the need for development of custom heterobifunctional recombinant antibodies, the previous solution to problems (i), (ii), and (iii); large molecules which also have the problem of variable and unpredictable degrees of internalization into target cells and tissues. This particular delivery system if coupled to the SSTR-2 receptor gene (or other safe reporter gene system) has the potential to non-invasively target a variety of receptors and cellular anti-



Fig. 2. Assembly of complexes for radionuclide imaging. Docking tag is fused to a targeting protein without affecting targeting epitopes. Radionuclide chelator is conjugated to a standardized adapter protein and loaded with $^{99\text{m}}\text{Tc}$. Appropriately designed, humanized adapter/docking tag system will be "non-destructive" for targeting proteins, and allow the use of multiple existing and newly discovered targeting proteins in a rapid and uniform fashion. [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

gens, selectively expressed within sites of interest, with high specificity and low background.

Gamma-aminobutyric acid (GABA_A)–Benzodiazepine Receptor Agonists

GABA is the most abundant inhibitory transmitter in the central nervous system (CNS) and is distributed within GABAergic neurons throughout the brain [Nutt and Malizia, 2001]. When GABA inhibitory activity exceeds that of excitatory inputs (mainly glutamatergic) sedation, amnesia, and ataxia appear. Benzodiazepines work by potentiating the effects of GABA on the chloride ion channel of GABA_A–benzodiazepine receptor complex. Benzodiazepine derivatives [¹¹C]flumazenil for PET and [¹²³I]iomazenil for SPECT that primarily image the peripheral (as opposed to central) benzodiazepine receptors are commercially available and have been applied to the neuroimaging of a variety of neurologic disorders including anxiety and temporal lobe epilepsy characterized in part by decreases in GABA_A receptors within the brain [Matheja et al., 2001; Hammers et al., 2002; Sata et al., 2002; Sauvageau et al., 2002]. In addition reductions in temporal-mesial uptake of [¹²³I]iomazenil can be found in regions that are structurally intact by MRI in patients with medically refractory temporal lobe epilepsy. It is now recommended that presurgical studies with [¹²³I]iomazenil (SPECT) or [¹¹C]flumazenil (PET) be performed as part of routine imaging along with MRI.

Interestingly, iomazenil also binds selectively to activated microglial cells (brain macrophages) that have no significant binding of tracer in their quiescent state. These cells also make up 1 out of 10 cells in the normal brain. Activated microglial cells are found in abundance with the brain (entorhinal, temporoparietal, and cingulate cortex) of patients with Alzheimer's presenile dementia and multiple sclerosis and can be readily imaged, quantified, and serially followed with [¹²³I]iomazenil SPECT or [¹¹C]flumazenil PET imaging [Cagnin et al., 2001; Debruyne et al., 2003; Versijpt et al., 2003].

Dopamine Transporter (DAT) and D2 Dopamine Receptor Imaging

The pre-synaptic DAT and the post-synaptic D2 receptor are two of the most extensively studied neurotransmitter-receptor systems in the CNS [Bergstrom et al., 1998; Voruganti

et al., 2001]. Several disease states, including depression, the antipsychotic drug induced negative syndrome of schizophrenia, Parkinson's disease, and extrapyramidal Parkinson-plus neurodegenerative syndromes are characterized by focal or regional decreases in DAT and D2 receptor binding [Ilgin et al., 2001; Prunier et al., 2001; Winogrodzka et al., 2001; Wong, 2002]. Opiates and Parkinson's disease have both been shown to effect the DAT system with SPECT imaging using two novel radiopharmaceuticals; [¹²³I]β-CIT, a cocaine analog with a binding constant of 1.6 nM for the DAT and [¹²³I]FP-CIT, a tracer that has been successful at documenting the accelerated pre-synaptic dopaminergic degeneration found in Parkinson's patients [Marek et al., 2003]. Diseases characterized by abnormal increases in D2 receptor binding potential include attention order-deficit-hyperactivity disorder (ADHD), mania, and schizophrenia. ¹²³I-iodo-benzamide (IBZM) or ¹²³I-iodolisuride (ILIS) (lisuride, an ergolene derivative used in the treatment of Parkinson's disease, *k* = 0.27 nM similar to 76Br-bromolisuride used for PET) SPECT. These studies all show excellent correlations of D2 binding potential with neuropsychiatric function and may have an immediate benefit in the diagnosis and treatment of depression associated in over a third of patients undergoing anti-psychotic treatment for schizophrenia.

One fascinating area of clinical research with DAT and D2 imaging agents has been the study of substance abuse [Volkow et al., 2003]. Abuse of cocaine, methamphetamine, methylenedioxy-methamphetamine (MDMA), alcohol, opiates, tobacco, marijuana, and inhalants all appeared to be associated with abnormalities of the brain dopamine system, the primary force behind the reward center in humans. Dopamine producing cell bodies are located in the midbrain within the substantia nigra and the ventral tegmental area with projections to the striatal area that is known as the reward center, the nucleus accumbens. All abused substances despite different mechanisms of action serve to increase synaptic levels of dopamine. Chronic substance abusers have stimulant-induced highs associated with increases in brain dopamine but abnormally low numbers of dopamine D2 receptors at rest as measured by the PET radioligand ¹¹C-raclopride [Doudet et al., 2003]. ¹¹C-raclopride is a radiopharmaceutical that binds to the post-synaptic D2/3 receptors and therefore is an

indirect indicator of endogenous concentrations of dopamine. This effect coupled to decreases in dopamine release in response to chemical stimuli leads to the compulsive drug seeking behavior in chronic substance abusers and is an active area of neuro-psychiatric investigation.

Estrogen and Progesterone

Evaluating the status of estrogen receptors can be helpful in defining a treatment strategy in patients with breast cancer. In the absence of imaging, receptor status is estimated by multiple biopsies of the primary tumor and regional lymph nodes [Rose et al., 1985]. Both fluorine (F)-18 estrogen analogs [McGuire et al., 1991] and iodinated compounds have been synthesized for PET imaging [Rijks et al., 1998]. An iodinated estrogen analog, 123-labeled cis-11beta-methoxy-17alpha-iodovinyl estradiol, was successful in the determination of estrogen receptor status in a study of 22 women with primary breast carcinoma using both planar and SPECT radionuclide imaging [Bennink et al., 2001]. Progesterone receptor SPECT imaging with a progesterone analog, Z-[¹²³I]IPG2, may also be possible in near future [Rijks et al., 1998].

Imaging of the $\alpha_v\beta_3$ Integrin

The integrins, a family of heterodimeric endothelial cell membrane proteins, serve as adhesion receptors for extracellular matrix proteins that contain exposed arginine, glycine, and, aspartate (single letter coding RGD) amino acid sequences [Ruoslahti and Engvall, 1997]. These include laminin, fibronectin, collagens, and vitronectin that help form blood vessels. The most abundant integrin expressed on the surface of proliferating endothelial cells is the $\alpha_v\beta_3$ receptor [Brooks et al., 1994]. In the adult human the $\alpha_v\beta_3$ integrin has a limited tissue distribution. It is not expressed on quiescent epithelial cells and appears at minimal levels on smooth muscle cells. In contrast, both activated endothelial cells in tumor capillaries [Eliceiri and Cheresch, 1999], and some tumor cells [Cheresch, 1991] express high levels of $\alpha_v\beta_3$.

The cyclic pentapeptide cyclo(-Arg-Gly-Asp-D-Phe-Val-) has been identified as a potent ($k_d < 10$ nmol/L) inhibitor of $\alpha_v\beta_3$ integrin binding to extracellular matrix proteins [Pfaff et al., 1994]. Modifications of this peptide at position four or five have allowed radiolabeling with iodine for SPECT, and F-18 for PET imaging [Haubner et al., 2001]. Contrast between tumor

and normal tissues (especially liver) has been since improved by addition of sugar to the amino acids of the peptide [Haubner et al., 1999]. Radiolabeled RGD-peptides have been recently used to image $\alpha_v\beta_3$ expression in tumor prior to the administration of $\alpha_v\beta_3$ antagonists such as EMD-121974 to allow selection of patients entering clinical trials. These peptides in near future will be used to assess the effectiveness of $\alpha_v\beta_3$ integrin blockade by specific doses of other $\alpha_v\beta_3$ antagonists. This approach will permit optimization of dose for a specific patient and tumor type.

Hypoxia

Angiogenic factors, including vascular endothelial growth factor (VEGF), are induced by tissue hypoxia [Brogi et al., 1994]. The amount of tumor hypoxia may therefore be related to the amount of angiogenesis. One of the effects of successful anti-angiogenic drug therapy is a reduction of blood supply to the tumor, which increases hypoxia. Hypoxia imaging can therefore be used in two different ways: to study angiogenesis itself and to determine the efficacy of drugs. Nitroimidazoles are a class of compounds that undergo biochemical reduction forming covalent bonds to intracellular protein thiols thus trapping the tracer in viable cells with abnormally low oxygen concentrations [Chapman et al., 1983]. In normoxic conditions however, these compounds enter and freely leave the cell unmodified thus distinguishing normal from hypoxic tissues. Misonidazole analogs and 2-nitroimidazole analogs have been labeled with ¹²³I and ^{99m}Tc for SPECT, and F-18 for PET imaging of hypoxia. These agents have demonstrated increased uptake in hypoxic and low flow ischemic myocardium and brain as well as in tumors [Parliament et al., 1992; Ballinger et al., 1996; Cook et al., 1998; Melo et al., 2000; Markus et al., 2002; Tolvanen et al., 2002; Hoffend et al., 2003; Song et al., 2003]. ^{99m}Tc labeled HL91 and BRU 59-21 as well as F-18 labeled fluoromisonidazole (¹⁸F-FMISO) have been recently used to study temporal changes in tumor hypoxia in patients undergoing radiation and chemotherapy for primary and recurrent squamous head and neck carcinoma [Rischin et al., 2001; Van De Wiele et al., 2001; Hoebbers et al., 2002].

Imaging Apoptosis

Apoptosis, also known as "programmed cell death", was named for the series of character-

istic energy dependent biochemical and morphologic changes that a cell undergoes as it commits to its own destruction and removal [Allen et al., 1997]. One of the earliest detectable changes in the apoptotic cascade is the externalization of phosphatidylserine (PS) due to the enzymatically controlled redistribution of PS from the inner to outer leaflet of the plasma membrane phospholipid bilayer [van Engeland et al., 1998]. Annexin V, an endogenous human protein, binds specifically to membrane bound PS, which is externalized on the cell surface [van Heerde et al., 1995]. Annexin V, because of its nanomolar affinity for PS, has been used in the flow cytometric detection of apoptotic cells in vitro, in vivo in animal models, and most recently in humans for the detection apoptosis and necrosis found in acute cardiac transplant rejection [Narula et al., 2001], tumor response to chemotherapy [Belhocine et al., 2002], and acute myocardial infarction [Thimister et al., 2003]. While annexin V has been labeled with ^{99m}Tc for SPECT imaging in humans, in near future it should be possible to label annexin V with ^{18}F , allowing higher resolution PET imaging, or via the substitution of ^{94m}Tc (a positron-emitting Tc isotope) using existing ^{99m}Tc protein labeling technologies [Tanaka et al., 1996].

MR techniques can also be used to directly detect apoptosis using suppressed lipid proton spectroscopic pulse sequences that can detect cells undergoing apoptosis both in vitro [Blankenberg et al., 1997] and in vivo [Hakumaki et al., 1999]. Cells undergoing apoptosis have an associated increase in membrane and cytoplasmic neutral mobile lipid droplets composed of polyunsaturated fatty acids, cholesterol esters, and triglycerides [Al-Saffar et al., 2002; Ferretti et al., 2003]. Outside the brain, however, water suppressed lipid proton MR spectroscopy remains a challenge due to physiologic motion and the non-specific "bleeding in" of lipid signal from adipose tissue as well as the low signal to noise and relatively poor spatial resolution of the technique.

Imaging of Cellular Stress With Annexin V

New data suggest that the PS expression can occur with non-lethal cell injury prior to the irreversible morphologic changes such as DNA fragmentation [Lejeune et al., 1998; Hammill et al., 1999; Furukawa et al., 2000; Lin et al., 2000; Maiese and Vincent, 2000; Martin et al.,

2000; Geske et al., 2001; Yang et al., 2002]. These in vitro studies showed that intermediate levels of PS exposure were noted in cells with no other morphologic features of apoptosis could be readily reversed upon removal of physiologic stressors such as nitric-oxide, p53 activation, allergic mediators, and growth factor deprivation. Studies of the surfaces of tumor endothelial cells also showed that PS expression could be reversibly increased by exposure to hypoxia/reoxygenation, acidity, thrombin, inflammatory cytokines, and hydrogen peroxide, all factors that are variably present in tumors, without inducing apoptosis [Ran et al., 2002]. Annexin V could therefore be useful as an imaging marker of tumor vessels. Thimister's clinical study found that annexin V localization partially resolved by day 3–4 and completely by day 8 in regions of ischemic injury following acute myocardial infarction [Thimister et al., 2003]. These results suggest that either injured cells that concentrated tracer were removed from the ischemic zone or the recovery of these cells in terms of both function and viability with loss of PS positivity. The reduction of perfusion abnormalities with restoration of regional wall motion 1 week following infarction suggests the latter explanation. If true then annexin V imaging maybe vastly more sensitive to cellular stress than previously thought and maybe a true marker of tissues at risk that have the potential for salvage with prompt therapeutic intervention [Strauss et al., 2000; Narula and Strauss, 2003].

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